

SZLOVÁKIAI MAGYAR AKADÉMIAI TANÁCS

Fiatal kutatók a szlovákiai magyar tudományosságért díj



SZMAT

Bioüveg – kalcium foszfát kompozit cementek elkészítése és tanulmányozása

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Background

<u>1.9.2012 - 24.8.2016</u>/ Institute of Materials Research of the Slovak Academy of Sciences (IMR SAS)



PhD. Student, Field of study: Materials Science and Engineering.

<u>2003 - 2006</u>/Pavol Jozef Šafárik University in Košice (UPJŠ)



Faculty of Science, Field of study: organic chemistry "Master's Degree"

2003 - 2006 / Pavol Jozef Šafárik University in Košice (UPJŠ)



Faculty of Science, Field of study: chemistry "Bachelor's degree"

<u>1999 - 2003</u> /Secondary school for medical assistants in Košice



Field of study: pharmaceutical assistant

Outline - IMR SAS

- > Advanced powder technologies/materials
- Nano-structured materials
- Structural and fuctional ceramics
- Advanced steels



Experimental equipments



FTIR Shimadzu IRAffinity1





JEOL JEM 2100 F UHR

JEOL FE SEM JSM-7000F XRD Phil



AURIGATM CrossBeam[®]: GEMINI[®] electron beam SEM



Biomaterials

synergistic interaction of <u>materials science</u>, <u>biological science</u>, <u>chemical science</u>, <u>medical science</u> and <u>mechanical science</u>

..... number of definitions

synthetic or natural materials to be used to replace parts of a living system or to function in intimate contact with living tissues (NIH)







amorphous glasses consisting solely of elements found in the body materials that are specially developed for the repair and reconstruction of diseased or damaged parts of the musculo-skeletal system

Biocements (CPC)



1980-Brown, Chow, LeGeros

mixture of one or more calcium phosphate powders which upon mixing with liquid phase sets in vivo at body temperature

PhD Thesis " Effect of bioactive glass addition on properties of calcium phosphate composite systems"

Applications

http://rotamed.com/en/index.php?option=com_conten t&view=article&id=87&Itemid=106



reinforcement of osteoporotic bones



http://buildingindustry.org/web







filling bone defects, connecting bone fragments

filling root canal, periodontal defects, dental pulp





https://asps.confex.com/asps/2003am/techprogram/images/3389-0.gif

craniofacial and maxillofacial applications



- 1) Synthesis of bioactive glasses by means of precipitation method
- 2) Characterization of chemical composition, phase evolution and particle morphology as well as clarification of precipitation mechanism of prepared glass systems

http://www.primogroup.de/de/produkt/fireandice

3) Preparation and characterization of composite bone cements based on brushite with the addition of binary CaO-SiO₂ and ternary CaO-SiO₂-P₂O₅ bioactive glass systems of different crystallinity.

1) Synthesis of BG



Sol-gel precipitation method



hydrated calcium silicate and calcium silicate phosphate (CSH/CSHP)



1. System "final pH 12.3" Ca/Si = 1



- diff. chem. composit.
- phase composition
- morphology

Mechanism of precipitation and phase composition of CaO-SiO2-P2O5 systems synthesized by sol-gel method

Journal of Non-Crystalline Solids (2015)



- 1. System "final pH 11.4"
- 2. System "final pH 10 con."
- 3. System "final pH 7.4"
- 4. System "final pH 5.5"

2) Preparation of cement composites



3) XRD analysis of biocements after hardening



4) FTIR analysis of biocements after hardening



5) Microstructure of biocements after hardening



6) Compressive strength of bioc. after hardening

10%CSH/B (a) 10%CSPH/B (b) 70 strength (MPa) 50 Compressive strength (MPa) 10% woll/B 30%CSPH/B 30%CSP/B 30%CSH/B 60 50%CSPH/B 30% woll/B 40 50%CSP/B 50% woll/B 50 30 40 Compressive 30 20 20 10 10 0 n 1 d 7 d 1 d 7 d Time (days) Time (days)

 $CaO-SiO_2$ / brushite

 $CaO-SiO_2-P_2O_5$ / brushite



7) Setting time of biocements after hardening

Optimum P/L ratio, final setting times total porosity

$CaO-SiO_2$ / brushite

Sample	P/L (mg/ml)	Final sett. time (min)	Porosity (%)
10CSH/B	2.50	12 ± 1.4	45 ± 1.7
30CSH/B	2.00	43 ± 2.8	58 ± 1.1
10woll/B	2.80	8 ± 1.8	45 ± 0.7
30woll/B	2.70	5 ± 2.1	44 ± 0.5
50woll/B	2.67	7 ± 0.7	44 ± 0.3

$CaO-SiO_2-P_2O_5$ / brushite

Sample	P/L (mg/ml)	Final sett. time (min)	Porosity (%)
10CSPH/B	2.22	25 ± 1.1	46 ± 0.3
30CSPH/B	1.70	20 ± 1.0	60 ± 0.6
50CSPH/B	1.21	17 ± 0.7	64 ± 0.4
30CSP/B	3.14	28 ± 1.4	64 ± 0.4
50CSP/B	3.18	30 ± 2.1	43 ± 0.8



Setting time

<u>Vicat aparatus</u>	<u>Guo et al.</u>
(ISO standard 1566)	CaSiO ₃ /CPC \rightarrow 5-20%, 21-30 min
The cements were considered set until the Vicat needle (400 g) no longer leaves a visible print on the surface of the pastes	$\frac{Huan and Chang}{Ca_3SiO_5/\beta - TCP/MCPM}$ $\frac{Wang \ et \ al.}{\beta - Ca_2SiO_4/ACP/DCPD}$ 8%, 42 min

8) In vitro cytotoxicity of biocomposites

Relative proliferation osteoblast activities and viability on composite substrates



<u>MTS assay:</u> is a colorimetric assay for assessing cell metabolic activity

...enzymes are capable of reducing the yellow tetrazolium dye to its insoluble formazan, which has a purple color. Determination of formazan in wells at a wavelength of 490 nm

120 2 days 9 days (c) 100 ABS/ABS standard (%) 80 60 40 20 10% 30% 50% 30% 50% standard CSPH/B CSPH/B CSPH/B CSP/B CSP/B CSH,CSPH 10 wt% 📫 ~ 70% prolif 10woll/B 0 % viability and prolif. cytotoxic ~ 20% prolif. 50woll/B \rightarrow increase of prolif. from ~ 40% to 70% after 9 d cultivation

 $CaO-SiO_2-P_2O_5$ / brushite

9) Morphology and osteoblast density

Morphology and osteoblast density on composite substrates after 9 d culture



10) Variations of pH and concentrat. of elements



11) Surface microtexture of biocomposites

Microstructure of composite substrates after 9 d cultivation



Conclusions

- Composite cements were prepared by mechanical mixing of CaO-SiO₂ and CaO-SiO₂-P₂O₅ systems of different crystallinity with brushite as calcium phosphate source of the cmenet matrix. The results showed a significant effect bioactive glass addition on the properties of calcium phosphate composite systems
- The phase composition in the final cements and transformation of brushite to calcium deficient hydroxyapatite were controlled by the Ca/P ratio in the initial cement powder mixture and by dissolution of calcium silicate and calcium phospho-silicate phase.
- Setting time of cement composites were in the range of 5-43 minutes depending on the bioactive glass content and the rate of transformation of the origin brushite phase.
- The compressive strength of the set cements increased with the filler addition and the highest value (exhibited composite cements with 50 wt% crystalline phase content.
- A strong relationship between the composite in vitro cytotoxicity and surface microtopography was demonstrated. The rougher microstructure and plate like morphology of coarser particles in cements allowed cells to better adhere and proliferate contrary to other samples with particles in the form of nanoneedles or thin plates perpendicularly oriented to sample surface.

Future perspective





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Thin Film Physics Department

The goal of research:

Electrospray deposition (ESD) of bioactive calcium phosphate thin films on Ti substrates



